Pompa

[54] METHOD AND APPARATUS FOR LOCATING AN IDEAL SITE FOR A DENTAL IMPLANT AND FOR THE PRECISE SURGICAL PLACEMENT OF THAT IMPLANT

[75] Inventor: Daniel G. Pompa, Roslyn Heights, N.Y.

[73] Assignee: Howard C. Weitzman, Woodmere, N.Y.; a part interest

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[52] U.S. Cl. ........................................... 433/76; 433/214; 433/215; 434/270; 434/263
[58] Field of Search ................................ 433/75, 76, 213, 214, 433/215, 173; 434/263, 270

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Primary Examiner—Gene Mancene
Assistant Examiner—Tod E. Manahan
Attorney, Agent, or Firm—Collard & Roe

ABSTRACT
An apparatus and method for locating and surgically positioning a hole for an implant and holder in a jawbone of a patient includes constructing a model of a jawbone. A structure is located within the model depicting variations in density within the jawbone. A hole is drilled into the model based on the location of the structure. A rod is placed into the hole and a guide template is fabricated around the model which forms a bore around the rod. The guide template is placed onto the jawbone of the patient and a hole is drilled through the bore into the jawbone to make a hole in the jawbone along the same path as the hole in the model for receiving the implant and holder.

17 Claims, 3 Drawing Sheets
METHOD AND APPARATUS FOR LOCATING AN IDEAL SITE FOR A DENTAL IMPLANT AND FOR THE PRECISE SURGICAL PLACEMENT OF THAT IMPLANT

BACKGROUND OF THE INVENTION

1. Field of the Invention

The present invention relates to a method and apparatus for locating a site and surgically positioning a dental implant. More specifically, it relates to a method and apparatus for placing an endosseous dental implant into the most optimal bone structure of a patient's upper or lower jawbone utilizing a surgical guide template that is fabricated with the use of computerized tomography and stereolithography.

2. The Prior Art

In the field of dentistry, tooth implants are increasingly being utilized. In the articles "Predictable Mandibular Nerve Location — A Clinical Zone of Safety" by Misch and Crawford, appearing in Dentistry Today, December, 1990, p. 32, and "Presurgical Prosthetics and Surgical Templates" by Zinner, Small and Panno, appearing in Dental Clinics of North America (Vol. 33, No. 4, October, 1989); and the U.S. Pat. No. 5,015,183 to Penick describe the present state of the art regarding the placement of oral implants with a surgical template and the inherent restrictions and limitations thereof. A problem in the art and science of placing dental implants is finding and locating sufficient bone structure in height, length and width in which to fix the implant so as to obtain the most optimum long term success. In general, the longest length implant that can be placed into the greatest dimensions of bone will give the best long term prognosis. An inherent problem exists with placing an implant into the human lower jaw. The alveolar nerve (Cranial Nerve V, Division III) passes through a canal entering the posterior area of a human jaw and coursing through it. As a result, a surgeon is limited by the depth to which he can place an implant and presently will stay safely above the nerve, as discussed in detail in the article "Predictable Mandibular Nerve Location — A Clinical Zone of Safety." This zone of safety restricts the surgeon to only utilizing approximately one-third to one-half of the full height of available bone depending on individual anatomical variation. If an implant impinged upon the nerve, the patient could lose feeling in their lower lip and chin on the affected side. Since the location of the nerve is difficult to pinpoint during the surgical procedure with present technology, the longer more desirable types of endosseous implants generally are not used in the area of the posterior lower jaw.

If an implant could be placed in the lower posterior jaw and engage the lower portion (inferior border) this would result in improved long term prognosis. The resulting implant could be twice the length achieved by present technology.

Presently, to place an implant into the inferior border of the posterior mandible (lower jaw) it is necessary to perform a nerve transposition procedure. This involves the dissection of the nerve from its canal, followed by placing the implants. Then the nerve is repositioned around the implants. The morbidity associated with this procedure is significant. (Howard Davis, D.D.S., 1992 August, American Association of Periodontics, Chicago, Illinois—Clinical Meeting.)

Alternatively, the surgeon could use the information on a standard C.T. scan and approximate the angle of the site for the implant. However, this method presents a risk of damage to the inferior alveolar nerve which can result in altered or no sensation to the lip and chin on the affected side. The worse case scenario is an irreversible loss of feeling to the lower lip, chin and gum tissue on that side. There is a large margin for error with this method due to a lack of precision in achieving the correct angle to direct the bur during the surgical procedure of placing the implant. Also known from the prior art are stereolithographic models (SLA Models) constructed from digital image data (computerized tomography) which allows the surgeon to view the external and internal anatomy prior to surgery, as described in the article entitled "Stereolithographic Models for Surgical Planning: Preliminary Report" by Stoker, Mankovich and Valentino, J. of Oral and Maxillofacial Surgery, May 1992, p. 466-471. However, stereolithographic models have not been used to place dental endosseous dental implants into the most optimal jawbone location and have not been used to specifically avoid contacting the inferior alveolar nerve and more specifically to actually bypass this structure thereby engaging the lowermost portion of the jaw.

This SLA Model also gives the operating surgeon the precise information (optimal height, length and depth of bone) that is needed to fabricate a specially designed surgical template to be used in any area of the upper or lower jaw.

SUMMARY OF THE INVENTION

It is therefore an object of the present invention to provide a method and apparatus for locating a site and surgically positioning a dental implant which overcomes the drawbacks of the prior art and allows more accurate and precise placement of dental implants. It is a further object of the present invention to reduce the risk of morbidity following the placement of an implant.

It is still a further object of the present invention to select the most ideal location with respect to the length and diameter for a dental implant.

It is still another object of the present invention to provide a path for the implant which avoids the inferior alveolar nerve in the lower jaw.

It is still another object of the present invention to provide a method and apparatus for drilling a bone along a predetermined trajectory into the most optimal bone structure of an upper or lower jaw.

These and other related objects are achieved according to the present invention by a method and apparatus for locating and surgically positioning a hole for an implant and holder in a jawbone of a patient to avoid a vital structure or structures, i.e., a sensory nerve (Cranial Nerve V, Division III), or engage a bone structure. The apparatus according to the invention for directing a bur includes a jawbone model formed by a method of scanning the jawbone with computerized tomography and constructing a stereolithographic model including a radiopaque (marker) representing the inferior alveolar nerve. The apparatus also includes a means for locating and drilling a hole in the model to avoid the radiopaque marker and a simulated implant (implant analog) is placed into the hole. A holder is then placed into this implant analog and protrudes above this implant analog. Then a guide template is fabricated on the
jawbone model including a bore formed around the
holder so that when the template is now transferred and
placed on the jawbone of the patient, a specifically
designed drill is guided by the template bore into the
jawbone along the same path as the hole in the model to
avoid the nerve and forms a hole for receiving the ac-
tual implant and holder. Alternatively, the apparatus
also includes a means for locating and drilling a hole in
said model to precisely engage a specific bony struc-
ture.

The apparatus also includes a surgical guide ring
having a cylindrical body with two ends. An outwardly
extending flange is located at one end of the surgical
guide ring with an aperture extending along the central
axis of the cylindrical body from one end to the other
end. The surgical guide ring is placed within the bore of
the guide template to further guide the drill, giving a
higher degree of accuracy and less margin for error.
The surgical guide ring is to be used with the SLA
generated surgical guide template to allow an implant to
engage optimal bone structure in any location of the
upper (maxillary) or lower (mandibular) jaw.

BRIEF DESCRIPTION OF THE DRAWINGS

Other objects and features of the present invention 25
will become apparent from the following detailed de-
scription considered in connection with the accompa-
nying drawings which disclose an embodiment of the
present invention. It should be understood, however,
that the drawings are designed for the purpose of illus-
tration only and not as a definition of the limits of the
invention.

In the drawings, wherein similar reference characters
denote similar elements throughout the several
FIG. 1a is a top plan view of a model of a jawbone;
FIG. 1b is a left side elevational view of the model;
FIG. 2a is a top plan view of the model showing
proposed implant sites;
FIG. 2b is a top plan view of an X-ray of the model
from FIG. 2a with an opaque marker and implant ana-
logs in place;
FIG. 3 is a side-elevational view of the model with
implants, holders and template;
FIG. 4a is an enlarged perspective view of a surgical
guide ring;
FIG. 4b is an enlarged perspective view of an alter-
mate embodiment of a surgical guide ring;
FIG. 5 is an exploded view of a jawbone, template,
guide rings and bur; and
FIG. 6 is a perspective view showing the template
with guide rings held in place by a holder.

DETAILED DESCRIPTION OF THE
PREFERRED EMBODIMENT

Referring now to the drawings and, in particular, FIGS. 1a and 1b, there is shown a stereolithographic
(SLA) model 10 of a human jawbone. A computed
tomography (CT) scan is performed on the individual
requiring a dental implant. The information from the
scan can then be processed to generate a clear acrylic
model 10 showing both interior structures and exterior
contours. The stereolithographic process is discussed in
detail in the article, "Stereolithographic Models for
Surgical Planning: Preliminary Report" by Stoker,
Mankovich and Valentino which appears in the Journal
of Oral and Maxillofacial Surgery, 50:466–471, 1992,
the subject matter which is incorporated by reference
into this patent.

Since the stereolithographic model displays both
outer contours and inner anatomic structures, a nerve
canal 11a is shown corresponding to the inferior alvoe-
lar nerve which is a radiolucent canal. The canal enters
the jaw on the inner aspect 11b (medial) and exits the
lower jaw on the outer aspect 11c (lateral) at the mental
foramen. A radiopaque marker 11d is placed into canal
11a, so that the location of the nerve can be easily seen
and X-rayed. Radiopaque marker 11d can be fabricated
from a twisted pair of 26 gauge stainless steel wire or a
pipe cleaner, for example. Other structures are present
in model 10 corresponding to radiopaque bony areas of
the jawbone.

As can be seen in FIG. 2a, when looking from the top
of model 10, a surgeon can easily locate radiopaque
marker 11d and sites 12, 13 and 14 can be drilled into
model 10 avoiding 11d. This is a technique known as
"model surgery" where surgery is performed on a model
of the patient prior to the actual surgery being
performed. Oral and Maxillofacial surgeons routinely
perform this procedure with other surgical endeavors,
I.e., orthognathic surgery. With the transparent model,
radiopaque marker 11d is easily visible and thus avoid-
able. With the present information, the actual operating
surgeon will perform the model surgery and educa-
tional "hands on" programs will be offered. The SLA
generated model also reveals to the surgeon where
deformities exist so that the surgeon can carefully plan
what areas may be augmented (grafted) prior to sur-
gery, as a separate procedure or at the same time the
implants are placed.

Model surgery is then performed on the SLA model
with the marker in place. Site 14, the most anterior site
is placed just medial (lingual) of the mental foramen.
It is also placed in a vertical plane 15 which passes
through the mental foramen and is generally perpendic-
ular to the surface of the model above and/or below the
mental foramen. Since the nerve 11a exits laterally at
outer aspect 11c, site 14 is in a relatively safe position.
Sites 13 and 12 are placed toward the posterior mandi-
ble. When placing the bur channel, the surgeon can
visualize radiopaque marker 11d within model 10 in
dimension. After drilling, the sites are fitted with the
implant analogs 22, 23 and 24. Implant analogs 22,
23 and 24 fit entirely within sites 12, 13 and 14. It should
be noted that implant analogs 22, 23 and 24 are radi-
opaque.

An X-ray, as shown in FIG. 2b, from above (occlusal
view) is then taken of model 10 to determine whether an
appropriate safety margin is established between radi-
opaque marker 11d and implant analogs 22, 23 and 24.
If any of the implant sites encroach marker 11d, then
that site will be adjusted away from marker 11d. A surgical
zone of safety of 2 mm is established as described in the
article "Predictable Mandibular Nerve Location—A
Clinical Zone of Safety" by Misch and Crawford. Sites
12, 13 and 14 can be alternately moved until all sites are
at least 2 mm away from opaque marker 11d and con-
firmed by X-ray analysis.

As can be seen in FIG. 3, implant analogs 22, 23 and
24 bypass radiopaque marker 11d which represents
nerve 11a, which was previously a boundary limiting
structure. Holders 32, 33 and 34 are then attached to
implant analogs 22, 23 and 24. Holders 32, 33 and 34
extend upwardly from implant analogs 22, 23 and 24
outside of sites 12, 13 and 14. A surgical guide template
16 is made, for example, from clear acrylic by placing it
around model 10 and holders 32, 33 and 34. Surgical
guide template 16 is made, for example, by Nealon's Technique (resin restoration) available from Fricke International, Illinois, or any other powder and liquid technique from model 10, and incorporates one or more guide paths for the bur. The guide path is formed by holders 32, 33, and 34 which extend along the longitudinal axis of implant analogs 22, 23, and 24 which are in sites 12, 13, and 14 through template 16. Guide template 16 is approximately 5 mm thick and can be used to aid in preventing the bur from developing its own path during actual surgery. The thickness of guide template 16 is determined by the exposed portion of holders 32, 33, and 34, i.e., the portion extending above model 10.

As can be seen in FIGS. 4a and 4b, the surgical guide rings 25a and 25b are additionally provided to improve the accuracy of the guide path of template 16. Guide rings 25a and 25b are made of hard material, which is resistant to chipping. The material can be fabricated from, for example, a titanium alloy, a chrome-cobalt alloy, or a titanium-chrome-cobalt alloy. Ideally, the material is titanium 6,4 (90% titanium, 6% aluminum, and 4% vanadium). Surgical guide rings 25a and 25b are provided with different internal diameters 27 and 28, but similar external diameters 26 which match that of the external dimension of holders 32, 33, and 34 and will therefore fit exactly in the hole (bore) created by these holders within surgical guide template 16.

Surgery is then performed on the patient. All this information including precise predetermined angulations can then be transferred to a surgical guide template, which is placed on the patient’s upper or lower jawbone.

FIG. 5 shows the completed guide template 16 which is now placed on the patient’s lower jawbone 20, not model 10. Surgical guide ring 25a is placed into a bore 38 of template 16 to provide a guide for drill or burr 17 as it penetrates jawbone 20. Burr 17 will follow the path of site 14 which was made during model surgery when the surgeon visualized the location of opaque marker 11d which represented nerve 11a, i.e., in a vertical plane which passes through the mental foramen and is generally perpendicular to the surface of the model above and/or below the mental foramen.

The first hole to be drilled is at site 14, having the greatest distance from nerve 11a, i.e., at site 14 with the largest safety margin. Initially, guide ring 25a having a smaller inner diameter is used along with a smaller burr to drill a pilot hole. Then surgical guide ring 25b and a corresponding larger burr can enlarge the hole. A series of surgical guide rings and burs may be used to enlarge the hole to a desired size. Since the surgical guide rings have the same external diameters, they can easily be substituted into the bores of guide template 16. Burs 17 are provided with markings along a lower cutting region 18 to indicate depth as the bur cuts into jawbone 20. (These markings are height adjusted to accommodate the depth of guide template 16 and guide ring 25.)

The surgeon can then read the depth right off of burr 17 without having to subtract the depth of template 16 and guide ring 25a. Above lower cutting region 18 is a stop 19 which limits the depth to which burr 17 can be inserted into jawbone 20.

As can be seen in FIG. 6, the first implant 24 is placed into the patient at site 14, followed by surgical holder 34 which is placed through template 16 and tightened to implant 24 to secure template 16 to jaw 20. This locks template 16 into place and increases the accuracy when subsequent holes, e.g., sites 13 and 12, are drilled corresponding to site 13 and site 12. The implants are provided with threads along their exterior and interior. The external threads may be self-tapping into jawbone 20 or a separate tap may be used prior to inserting the implant, based upon the jawbone density. Once implant 24 is inserted, the exterior threads of holder 34 are screwed into the internal threads of implant 24. Other holes are created, i.e., into sites 13, 12' with the use of guide rings and specialized burs and the implants are placed. The holders are removed from the implants and a cover screw is placed into each implant and the area is irrigated and closed. It should be noted that the implants, for example, titanium or titanium-alloy implants have a high degree of bone biocompatibility.

The implants, which are placed according to the invented described method, bypass the inferior alveolar canal and engage the inferior border of the mandible.

It should be noted that any surgical procedure requiring precise knowledge of optimal bone dimensional anatomy and any procedure performed in bone in the vicinity of a vital structure, i.e., nerve, artery, vein, etc., can benefit from the method and apparatus disclosed herein. In areas of the human upper (maxillary) and lower (mandible) jaw, other than the posterior lower (mandible) jaw, this method and apparatus can also be of a great advantage to the patient and surgeon. For example, in the maxillary jaw, there are a number of dense areas of bone (the pt ergodial plate convergence posterior to the maxillary tuberosity and the junction of the lateral nasal wall and medial antral wall) which in a severely resorbed upper (maxillary) jaw are the most ideal sites to engage. Up to the present time, the degree of accuracy and precision available to place implants into these areas is limited at best. With the STA Gener ated Model, a replica of the maxillary sinus wall, nasal wall and pt ergodial plates will be precisely replicated and as described in this invention, the operating surgeon can perform model surgery on a clear model and transfer that information to the guide template and follow the same method as described for precise and accurate placement into these sites. The ability to perform precise placement can actually result in a less significant surgical procedure. Many of these patients with a re sorbed maxillary upper jaw would need a pre-implant surgery to graft or augment the area and then have a second procedure performed to place the implants. The graft and augmentation procedure may be avoided with the ability to place implants with the precision described herein.

While only a single embodiment of the present invention has been shown and described, it is to be understood that many changes and modifications may be made thereunto without departing from the spirit and scope of the invention as defined in the appended claims.

What is claimed is:
1. A method for locating and surgically positioning a hole for an implant and holder in a jawbone of a patient comprising the steps of:
   i) constructing model of the jawbone including inner anatomic structures;
   ii) locating a structure within the model depicting variations in density within the jawbone;
   iii) drilling a hole into the model based on the location of the structure;
   iv) placing a rod into the hole;
v.) fabricating a guide template around the model and forming a bore around the rod; and
vi.) placing the guide template onto the jawbone of the patient and drilling through the bore into the jawbone to make a hole in the jawbone along the same path as the hole in the model for receiving the implant and holder.

2. The method according to Claim 1, wherein the rod includes a simulated implant analog and a holder.

3. The method according to Claim 2, wherein said step of constructing a model of the jawbone comprises: scanning the jawbone with a computerized tomography scan to create a computer image; tracing anatomical structures within the image; and constructing a stereolithographic model of the jawbone based on the anatomical structures and information reformatted from the computerized tomography scan.

4. The method according to Claim 3, wherein said step of locating a structure includes locating a structure within the model depicting a radiopaque bony area within the jawbone; and said step of drilling a hole includes drilling a hole in the model to penetrate and engage the structure.

5. The method according to Claim 3, wherein said step of locating a structure includes locating a structure within the model depicting a radiolucent canal within the jawbone, and said step of drilling a hole includes drilling a hole into the model to avoid the structure.

6. The method according to Claim 3, wherein said step of drilling a hole into the model and avoiding or engaging the structure includes verifying the position of the hole by radiographic analysis.

7. The method according to Claim 6, additionally including the step of: placing a surgical guide ring into the bore of the template, prior to the step of placing the template onto the jawbone of the patient.

8. The method according to Claim 7, additionally including the step of selecting a surgical guide ring having an internal diameter which is precisely machined to be slightly larger than the external diameter of a drill, so that the drill is accurately guided into the jawbone along the same path as the hole in the model that is created during model surgery prior to the step of placing a surgical guide ring into the guide template.

9. An apparatus for locating and surgically positioning a hole for an implant and holder in a jawbone of a patient comprising:

   a jawbone model including inner anatomic structures formed by a method of scanning the jawbone with computed tomography and constructing a stereolithographic model including a structure within said model depicting variations in density within the jawbone; means for locating and drilling a hole in said model based on the location of said structure; a rod placed into the hole; and a guide template disposed on said jawbone model including a bore formed around said rod so that when said template is placed on the jawbone of the patient, a drill is guided by said template bore into the jawbone along the same path as the hole in said model to form a hole for receiving the implant and holder.

10. The apparatus according to Claim 9, wherein said jawbone model is constructed from digital image data of the jawbone.

11. The apparatus according to claim 10, wherein said structure within said model depicts a nerve canal with the hole being drilled at least 2 mm away from said structure.

12. The apparatus according to claim 11, wherein said structure within said model depicts a dense bony area with the hole being drilled to engage said structure.

13. The apparatus according to Claim 11, wherein said jawbone model is created from a translucent material.

14. The apparatus according to Claim 11, additionally including a surgical guide ring having a cylindrical body with two ends, and an outwardly extending flange at one end thereof and an aperture located along a central axis of said cylindrical body extending from one end to the other end, wherein said surgical guide ring is placed within the bore of said guide template to further guide the drill.

15. The apparatus according to Claim 14, wherein said surgical guide ring is made of a hard material which resists chipping.

16. The apparatus according to Claim 15, wherein the material is selected from a group consisting of a titanium alloy, a titanium-coil alloy, or a titanium-chrome-cobalt alloy.

17. The apparatus according to Claim 16, additionally including a series of surgical guide rings having the same external diameter and varying internal diameters, each corresponding to a particular drill, the internal diameter of each guide ring is slightly larger than an external diameter of the corresponding drill.

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Refine Search  ref/5320529

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<thead>
<tr>
<th>PAT. NO.</th>
<th>Title</th>
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<td>Tooth-implant method and appliance</td>
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<tr>
<td>2 8,221,430</td>
<td>System and method for manufacturing arthroplasty jigs</td>
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<tr>
<td>3 8,221,121</td>
<td>Method for pre-operative visualization of instrumentation used with a surgical guide for dental implant placement</td>
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<tr>
<td>4 8,215,957</td>
<td>Dental implant placement locator and method of use</td>
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<td>5 8,206,153</td>
<td>Method for selecting implant components</td>
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<tr>
<td>6 8,186,999</td>
<td>System and arrangement for production and insertion of a dental bridge structure</td>
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<td>7 8,185,224</td>
<td>Method for manufacturing dental implant components</td>
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<td>8 8,160,345</td>
<td>System and method for image segmentation in generating computer models of a joint to undergo arthroplasty</td>
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<td>9 8,157,563</td>
<td>Guide device able to interact with a number of sleeves disposed in a tooth template</td>
</tr>
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<td>10 8,142,189</td>
<td>Arrangement and device for using a template to form holes for implants in bone, preferably jaw bone</td>
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<tr>
<td>11 8,118,597</td>
<td>Laterally inserted dental implant assembly and method for securing a dental prosthesis</td>
</tr>
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<td>12 8,083,774</td>
<td>Percutaneous vertebral fusion system</td>
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13 8,038,440 T Method for placing and manufacturing a dental superstructure, method for placing implants and accessories used thereby
14 8,011,927 T Method for pre-operative visualization of instrumentation used with a surgical guide for dental implant placement
15 7,988,449 T Healing components for use in taking impressions and methods for making the same
16 D642,263 T Arthroplasty jig blank
17 7,950,924 T Arrangement and device for using a template to form holes for implants in bone, preferably jaw bone
18 7,942,668 T Drill template arrangement
19 7,905,726 T Surgical guide for dental implant and methods therefor
20 7,845,943 T Method for making and using a template for locating a dental implant and components relating thereto
21 7,833,249 T Formable orthopedic fixation system
22 7,824,181 T Custom-fit implant surgery guide and associated milling cutter, method for their production, and their use
23 7,780,705 T Formed in place fixation system with thermal acceleration
24 7,774,084 T Computer-aided implantaing of orthodontic anchorage devices using surgical guides
25 7,771,476 T Curable orthopedic implant devices configured to harden after placement in vivo by application of a cure-initiating energy before insertion
26 7,758,345 T Systems and methods for design and manufacture of a modified bone model including an accurate soft tissue model
27 7,727,262 T Formed in place fixation system with thermal acceleration
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30 7,632,097 T Method for manufacturing a suprastructure and a corresponding drill jig
31 7,621,744 T Surgical guide for use during sinus elevation surgery utilizing the Caldwell-Luc osteotomy
32 7,601,156 T Limb lengthener
33 7,435,088 T Device for determining position
34 7,331,786 T Manufacturing a dental implant drill guide and a dental implant superstructure
35 7,153,132 T Mini-dental implant surgical stent
36 7,097,451 T Thermoplastic surgical template for performing dental implant osteotomies and method thereof
37 7,086,860 T Implant placement system
38 6,926,525 T Instrument for the parallel installation of dental implants
39 6,913,463 T Drilling guide for dental implantation
40 6,869,282 T Implant positioning device and method
41 6,814,575 T Manufacturing a dental implant drill guide and a dental implant superstructure
42 6,793,491 T Stabilizing implant system
43 6,755,652 T Method for producing dental restoration elements
44 6,672,870 T Method and instrumentation for attaching dentures
45 6,468,079 T Abrasive radiopaque endodontic marking tools and related methods
46 6,400,801 T Smooth radiopaque endodontic marking tools and related methods
47 6,296,483 T System for preparing the placing of a dental implant
48 6,224,373 T Simulation method for visualizing density of jawbone for dental implantation
49 6,155,825 T Radiopaque endodontic marking tools and related methods
50 6,099,313 T Dental implant, a template for inserting a dental implant, and a process for producing them
Results of Search in US Patent Collection db for:
**REF/5320529**: 66 patents.
*Hits 51 through 66 out of 66*

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<td>Dental implant distractor method and apparatus</td>
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<td>52 5,989,025 T</td>
<td>Drill guide</td>
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<td>53 5,967,777 T</td>
<td>Surgical template assembly and method for drilling and installing dental implants</td>
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<td>54 5,927,982 T</td>
<td>Three dimensional guidance system for dental implant insertion</td>
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<td>55 5,915,962 T</td>
<td>Dental implant and prosthesis positioning</td>
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<td>56 5,800,168 T</td>
<td>Adjustable guiding device for positioning dental implants, implantation system comprising it and method employing same</td>
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<tr>
<td>57 5,797,741 T</td>
<td>Dental implant article and device for fitting it</td>
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<tr>
<td>58 5,769,636 T</td>
<td>System for diagnosis, placement and prosthetic restoration of root form implant</td>
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<td>Methods for manufacturing a dental implant drill guide and a dental implant superstructure</td>
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<td>Drill guide kit</td>
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<td>Drill guide for dental implants and method</td>
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<tr>
<td>63 5,580,244 T</td>
<td>Method and apparatus for taking dental impressions</td>
</tr>
<tr>
<td>64 5,538,424 T</td>
<td>Radiographic depth and prosthetic positioning guide</td>
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http://patft.uspto.gov/netacgi/nph-Parser?Sect1=PTO2&Sect2=HITOFF&n=8/2/2012